



#### The webcast will start in a few minutes....

## Ground reaction force prediction

WITH THE ANYBODY MODELING SYSTEM







Morten Enemark Lund Application Engineer AnyBody Technology



## Outline

#### Introduction by the Host

#### GRF prediction in sports activities

• by Sebastian Skals

#### Technical explanation

• by Michael Skipper Andersen

#### Hands on:

- Adding GRF prediction to an existing Anybody MoCap model
- Questions and answers

#### Presenters:



Sebastian Skals, M.Sc. Research Assistant National Research Centre for the Working Environment Danish Ministry of Employment. Denmark



Michael Skipper Andersen, Ph.D. Associate professor Department of Mechanical and Manufacturing Engineering. Aalborg University Denmark



## Who is AnyBody?





#### <u>AnyBody Technology</u> (Aalborg, DK; Boston, US)

- AnyBody Modeling System
- Licenses, Training, Support
- Consulting

#### AnyBody Knowledge Centers

- DK: Aalborg University Prof. Rasmussen
  - Biomechanics, Ergonomics, Sport, Automotive
- US: Colorado School of Mines Prof. Petrella
  - Biomechanics, Orthopedics, Sport
- GER: OTH Regensburg Prof. Dendorfer
  - Biomechanics, Orthopedics, Gait









## Modeling with measured forces



Boundary conditions are necessary for inverse dynamic analysis.

In MoCap models this is provided by force plates.

What if **no measurements are available**?



## Ground reaction force prediction

#### IN SPORTS ACTIVITIES

Sebastian Skals, M.Sc. Research Assistant National Research Centre for the Working Environment Danish Ministry of Employment.





#### PREDICTION OF GROUND REACTION FORCES AND MOMENTS DURING SPORTS-RELATED MOVEMENTS

#### SEBASTIAN L. SKALS<sup>1</sup>, MOONKI JUNG<sup>2</sup>, MICHAEL DAMSGAARD<sup>2</sup>, MICHAEL S. ANDERSEN<sup>3</sup>

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## INTRODUCTION

Inverse Dynamic Analysis (IDA) of musculoskeletal models

- Applied in many fields, e.g., sports biomechanics
- Estimation of muscle, ligament, and joint forces
- 1) Top-down
  - Under-determinate during double support

#### 2) Bottom-up

- Force plate measurements
  - $\rightarrow$  Residual forces and moments





## INTRODUCTION

Typical solutions to these issues

- 1) Minimise residuals through optimisation methods
- 2) Estimate/distribute GRF&Ms under both feet

Proposed solutions for 2:

- Minimise joint moments (Audu et al. 2003, 2007)
  - Only standing positions, not movement
- Artificial Neural Network (Eel Oh et al. 2013, Choi et al. 2013)
  - Comprehensive analysis necessary to determine input
- Dynamic contact model and muscle recruitment (Fluit et al. 2014)



- Universal method
- Scaled model and kinematic data only
- Validated for activities of daily living

## INTRODUCTION

None of the existing methods have been validated for sports-related movements.

- Force plate measurements particularly limiting
- Larger accelerations and forces
- Complex movement patterns and contact conditions
- AIM: To evaluate the accuracy of the method of Fluit et al. (2014) to predict GRF&Ms during sports-related movements.
  - IDA of movements common for sports and recreational exercise



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- Compare predicted GRF&Ms to measured data
- Compare joint kinetics between models

### **EXPERIMENTAL PROCEDURES**

- Eight male and two female subjects (age: 25.70 ± 1.49 years, height: 180.80 ± 7.39 cm, weight: 76.88 ± 10.37 kg)
- Five sports-related movements:
  - Running at a self-selected pace
  - Backwards running
  - Side-cut
  - Vertical jump
  - Acceleration from a standing position (ASP)
- Varying force characteristics and double/single support





## **EXPERIMENTAL PROCEDURES**

Marker-based motion analysis:

- Eight infrared cameras sampling at 250 Hz (Oqus 300 series)
- Qualisys Track Manager v. 2.9
- Two AMTI force plates sampling at 2000 Hz
- 35 reflective markers
  - 29 placed on the body
  - 3 on each running shoe
- Data low-pass filtered at 15 Hz







### **MUSCULOSKELETAL MODELS**

Based on the *GaitFullBody* template from the AnyBody Managed Model Repository v. 1.6.3

Model scaling and kinematics

(Andersen et al. 2009, 2010)

- Adjusts segment lengths and marker coordinates
- Minimises the sum of marker residuals

#### **Inverse Dynamic Analysis**

- Twente Lower Extremity Model (Horsman et al., 2007)



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- Simple constant strength muscles
- Quadratic muscle recruitment



### **PREDICTION OF GRF&Ms**

Method of Fluit et al. (2014) adopted, but alterations were made in an attempt to improve the method.

- 18 contact points defined under each foot
- Five artificial muscle-like actuators in each contact point
- $F_{max}$ ,  $z_{limit}$ , and  $v_{limit}$  (contact parameters)
- Smoothing function implemented
- Solved as part of muscle recruitment algorithm















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0 50 100 Cycle [%]

V. JUMP LL



Cycle [%]

ASP RL

ASP LL



*r* ranging from 0.97 to 0.99, median 0.99

RED: Measured GRF&Ms BLUE: Predicted GRF&Ms Shaded areas: ± 1 STD † = sig. diff. peak forces

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r ranging from 0.13 to 0.96, median 0.61

RED: Measured GRF&Ms BLUE: Predicted GRF&Ms Shaded areas: ± 1 STD



V. JUMP RL











Cycle [%]











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r ranging from 0.69 to 0.95, median 0.87

**RED: Measured GRF&Ms BLUE: Predicted GRF&Ms** Shaded areas: ± 1 STD





V. JUMP RL H = 10 H = 10 S = 0S = 0

V. JUMP LL

50

Cycle [%]

0







0 50 100 Cycle [%]



#### r ranging from 0.86 to 0.95, median 0.94

100

RED: Measured GRF&Ms BLUE: Predicted GRF&Ms Shaded areas: ± 1 STD







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r ranging from 0.78 to 0.94, median 0.94

RED: Measured GRF&Ms BLUE: Predicted GRF&Ms Shaded areas: ± 1 STD **†** = sig. diff. peak forces

### DISCUSSION

- Comparable results for vertical GRFs, joint flexion moments, and resultant JRFs across all movements
- Majority of peak forces significantly different
  - Adjusting contact parameters a possible solution
- Discrepancies identified for, e.g., transverse GRM and HERM
  - Signal-to-noise ratio
  - Simple knee model (hinge joint)
- Areas to improve:
  - Foot-ground contact determination
  - More detailed knee and foot model
  - Sensitivity analysis on contact parameters



## **CONCLUSION AND FUTURE WORK**

- Could be used instead of force plate data
- Alternative to multi-setting instrumentation of force plates
  - Outdoor environments
  - Workplaces
  - Treadmills
- Combination with other motion analysis systems, e.g.,
  - Electromagnetic tracking systems
  - Accelerometers/gyroscopes
  - Marker-less systems, e.g., Sandau et al. (2014)
  - Interface between MLS and AnyBody (Skals et al. 2014)







#### PREDICTION OF GROUND REACTION FORCES AND MOMENTS DURING SPORTS-RELATED MOVEMENTS

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## How does it work?

#### Associate Professor Michael Skipper Andersen, PhD

Department of Mechanical and Manufacturing Engineering, Aalborg University, Denmark









## **Coulomb friction**

- Normal force is unilateral.
- Friction force and normal force are perpendicular.
- Friction force is limited by the normal force and friction coefficient.



$$f_n \ge 0$$
$$f_f \le \mu f_n$$





## **Muscle recruitment**

$$\min G(\mathbf{f}^{(m)})$$
  
s.t.  $\mathbf{C}\mathbf{f} = \mathbf{d}$   
 $\mathbf{f}^{(m)} \ge 0$ 

• Min/max:

$$G(\mathbf{f}^{(m)}) = \max_{i} \left( \frac{\mathbf{f}_{i}^{(m)}}{\mathbf{N}_{i}} \right)$$

• Polynomial:

$$G(\mathbf{f}^{(m)}) = \sum_{i}^{n} \left(\frac{f_{i}^{(m)}}{N_{i}}\right)^{p}$$
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## **Implementation: forces**



$$\mathbf{f}_{n} = \mathbf{f}^{1} + \mathbf{f}^{2} + \mathbf{f}^{3} + \mathbf{f}^{4} + \mathbf{f}^{5}$$
$$\mathbf{f}_{f} = \mu \mathbf{f}^{2} + \mu \mathbf{f}^{3} + \mu \mathbf{f}^{4} + \mu \mathbf{f}^{5}$$
$$\mathbf{f}^{i} \ge 0$$



## **Implementation: contact**

## **Contact when:**

- Node inside contact area.
- Node velocity small.





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## **Implementation: contact**

- Contact controlled with the "muscle" strengths
- Transitions are smoothed.
- Smoothing approaches:
  - Post-process kinematics.
  - Smoothing based on node position and velocity.















# Prediction of Ground Reaction Forces in Inverse dynamic simulations

#### MS Andersen<sup>1</sup> R Fluit<sup>2</sup>, S Kolk<sup>3</sup>, N Verdonschot<sup>2,4</sup>, HFJM Koopman<sup>2</sup>, J Rasmussen<sup>1</sup>

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7<sup>th</sup> World Congress of Biomechanics, Boston, 2014



## **Experimental data**

- Nine healthy subjects (4 males and 5 females)
- Gait lab data.
  - Full-body marker set (53 markers).
  - Six-camera Vicon system (100 Hz sampling).
  - Two AMTI forceplates (1000 Hz).
- Activities of daily living (ADLs):
  - Walking at comfortable (CWS) speed
  - Walking at a slow (CWS-30%) speed.
  - Walking at a fast (CWS+30%) speed.
  - Walking over a 10, 20 and 30 cm obstacle.
  - Gait initiation and termination.
  - Deep squatting (DS).
  - Stair ascent (SA) and descent (SD).









## Modelling

- The AnyBody Modeling System v. 5.3.1.
- New Twente lower extremity model (TLEM) v. 2.0. (Carbone et al, 2015).
- Hill-type muscle models.





Fluit et al. 2014. Prediction of ground reaction forces and moments during various activities of daily living. *J. Biomech.* 47(10), 2321–2329


## **Modelling: scaling**

- Segment length and marker location optimisation (Andersen et al. 2010).
- Performed on one gait trial per subject.



Produced with VideoMach www.videomach.com





### **Modelling: contact model**

- Coulomb friction model.
- Normal and static friction forces modelled with muscle-like actuators.
- 12 contact points under each foot.
- Ground contact when:
  - Node close to the ground plane.
  - Node velocity small.
- Transitions are smoothed by controlling the strength of the contact "muscle".
- Residual "muscles" on pelvis with low strength.





RESEARCH PROIECT



## **Modelling: inverse dynamics**

- Simultaneously computes the muscle, joint and ground reaction forces.
- Masses distributed according to Winter.
- Strength: Length-mass-fat scaling (Rasmussen et al., 2005).
- Recruitment criterion: Sum of muscle activitities cubed.







## Comparisons

#### • Variables

- GRF&M:
  - Force plate reference frame.
  - Equivalent GRM at the location of the ankle joint center projected onto the force plate.
- Joint moments.
- Metrics
  - Root-mean-square difference (RMSD).
  - Pearson correlation coefficient, ρ.
- Statistics
  - Two-tailed Wilcoxon signed rank test.
    - Mean GRF&M.
    - Peak GRF&M.







# **CWS results: GRF&M**













\*: significant difference in mean. †: significant difference in peak.



- Black, solid line: mean experimental data.
- Thin lines:  $\pm 1$  SD in the experimental data.
- Gray area: predicted mean ± 1 SD.

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## **Results: GRF&M**



- \*: Significant difference in mean.
- †: Significant difference in peak. p < 0.05

- Black, solid line: mean experimental data.
- Thin lines: ± 1 SD in the experimental data.
- Gray area: predicted mean ± 1 SD.



# **CWS results: Joint moments**



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#### **Conclusions**

- Generally, very good agreements between predicted and measured GRF&Ms were found.
- The prediction was poorest for the transverse GRM.
  - Likely caused by the hinge knee model.
- Potential applications:
  - Predictive models.
  - Measurement systems using inertial measurement units only.
  - Treadmill gait without force plates.
  - To improve dynamic consistency in inverse dynamic simulations.





### **Further reading**

- Fluit et al. 2014. Prediction of ground reaction forces and moments during various activities of daily living. *J. Biomech.* 47(10), 2321–2329
- Jung et al. 2014. Ground reaction force estimation using an insole-type pressure mat and joint kinematics during walking, *J Biomech*. 47(11), 2693-2699
- Skals 2015. Prediction of ground reaction forces and moments during sportsrelated movements, Master's Thesis, Aalborg University, Denmark





#### Thank you!

Michael Skipper Andersen, Ph.D. Associate Professor Department of Mechanical and Manufacturing Engineering Aalborg University <u>msa@m-tech.aau.dk</u>









[Enter a question for staff]

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ADDING GRF PREDICTION TO A MOCAP MODEL



Send

# Get the code...

- GRF prediction has always been possible AnyBody for long time, but it has not be easy...
- We have wrapped the code in AnyScript class templates to make it easy to use...

• Available on the wiki.anyscript.org

#### wiki.anyscript.org





# Time for questions:

#### wiki.anyscript.org



GFB prediction relies on conditional contacts added to the feet of the model. The conditional contacts work as force actuators to generate the normal and frictional forces necessary to balance model. Mathematically, the actuators are modelled similarly to muscles and the contact forces are determined by the muscle recruitment optimization.

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#### AnyBody events:

- Oct. 27<sup>th</sup> Webcast:
  - Title: Load Analysis of the hip joint for occupational activities
  - Presenter: Dipl.-Ing. Patrick Varady. Institute of Biomechanics, Trauma Center Murnau and Paracelsus Medical University Salzburg
- Oct. 26<sup>th</sup> to 30<sup>th</sup> HFES 2015 (Los Angeles)
  - Send us an email to schedule a meeting: sales@anybodytech.com

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